

## FSI with Application in Hemodynamics Analysis and Simulation

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A. Hundertmark (Uni-Mainz) Š. Nečasová (Academy of Sciences, Prague) G. Rusnáková (Uni-Košice/Uni-Mainz) • cardiovascular disease: "number 1 killer" in the Westen countries:





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 $\Longrightarrow$  importance of further detailed study e.g. using computational science







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- remove waste products
- defend the body against infection through the action of antibodies



play a vital role in fighting infection in the body





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the formation of blood clots (coagulation) is essential for large injuries

• properties of erythrocytes: (45%)





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  - ability to aggregate and form a branched 3D microstructure at low shear rates



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- properties of erythrocytes: (45%)
  - ability to aggregate and form a branched 3D microstructure at low shear rates
  - deformability
  - tendency to align with the flow field at high shear rates
- $\implies$  effect non-Newtonian behaviour of blood



### **Motivation**

#### Hemodynamic factors:

flow separation, flow recirculation, and oscillatory wall shear stress:

important role in the localization and development of vascular diseases  $\Longrightarrow$ 

- healthy patient: high shear rate, typical vessel lengths: no time to build microstructures

Newtonian models reasonable approximation



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- disease states: diseases in which the arterial geometry has altered (aneurysms), aggregates get more stable non-Newtonian models more relevant



Blood: plasma + cells (45% volume concentration)

vessel	radius	RE
aorta	1.25	3400
arteries	0.2	500
arterioles	1.5.10 <sup>-3</sup>	0.7
veins	0.25	140
vena cava	1.5	3300







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shear thinningviscoelasticity



Blood: plasma + cells (45% volume concentration)



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## Characteristic numbers



Reynolds and Wormesley number



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## Characteristic numbers

$$Re = rac{
ho \, U \, L}{\mu} \qquad lpha = rac{L}{2} \sqrt{rac{
ho \, \omega}{\mu}}$$

Reynolds and Wormesley number

$$\begin{array}{l} \rho \ldots \ \text{density; } 1.06 \times 10^{-3} \ \text{kg} \cdot \text{m}^{-3}, \\ U \ldots \ \text{characteristic velocity,} \\ \textbf{\textit{u}} = (u_1, \ldots, u_d) \ldots \ \text{fluid velocity} \\ L \ldots \ \text{characteristic length} \\ \mu \ldots \ \text{characteristic viscosity; } 3 - 5.5 \ \text{mPa} \cdot \text{s} \\ \omega \ldots \ \text{characteristic angular frequency} \\ \textbf{\textit{Re}} \in (0.0015, 6100) \qquad \alpha \in (0.003, 30) \end{array}$$



## Outline

#### Mathematical model Fluid equations

Structure equation Fluid-structure interaction

heoretical result Analysis





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## Fluid equations

shear-thinning properties

$$\rho \partial_t \boldsymbol{u} + \rho \left( \boldsymbol{u} \cdot \nabla \right) \boldsymbol{u} - \operatorname{div} \left[ 2 \mu (|\boldsymbol{D}(\boldsymbol{u})|) \boldsymbol{D}(\boldsymbol{u}) \right] + \nabla \pi = \mathbf{0}$$
  
div  $\boldsymbol{u} = \mathbf{0}$ 



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## Fluid equations

shear-thinning properties

$$p\partial_t \boldsymbol{u} + \rho \left( \boldsymbol{u} \cdot \nabla \right) \boldsymbol{u} - \operatorname{div} \left[ 2\mu(|\boldsymbol{D}(\boldsymbol{u})|)\boldsymbol{D}(\boldsymbol{u}) \right] + \nabla \pi = 0$$
  
 $\operatorname{div} \boldsymbol{u} = 0$ 

Carreau-Yasuda model

$$\mu = \mu(D(\boldsymbol{u})) = \mu_{\infty} + (\mu_0 - \mu_{\infty})(1 + \gamma |D(\boldsymbol{u})|^2)^{\frac{p-2}{2}}$$

Yeleswarapu model

 $\mu = \mu(D(\boldsymbol{u})) = \mu_{\infty} + (\mu_0 - \mu_{\infty}) \frac{\log(1 + \gamma |D(\boldsymbol{u})|) + 1}{(1 + \gamma |D(\boldsymbol{u})|)}$ 



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## viscoelastic properties

- blood:
  - ability to store and release energy (from its branched 3D structures)





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## viscoelastic properties

- blood:
  - ability to store and release energy (from its branched 3D structures)
  - challenge: developing nonlinear viscoelastic constitutive models for blood
  - the simplest model that captures the shear rate dependence and elasticity the rate-type shear thinning model (Oldroyd-B type model)

$$\tau = -\pi I + \tau^{\nu} + \tau^{e}$$

$$\lambda \left( \frac{\partial \tau^{\boldsymbol{e}}}{\partial t} + \boldsymbol{u} \cdot \nabla \tau^{\boldsymbol{e}} - \tau^{\boldsymbol{e}} \cdot (\nabla \boldsymbol{u})^{T} - \nabla \boldsymbol{u} \cdot \tau^{\boldsymbol{e}} \right) + \tau^{\boldsymbol{e}} = 2 \left( \frac{\mu(\boldsymbol{D}(\boldsymbol{u}))}{\mu_{0}} - (1 - \alpha) \right) \boldsymbol{D}(\boldsymbol{u})$$

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#### viscoelastic shear-dependent fluids

 $div(\mathbf{u}) = 0$ 

$$Re\left(\frac{\partial \mathbf{u}}{\partial t} + \mathbf{u} \cdot \nabla \mathbf{u}\right) = -\nabla \pi + (1 - \alpha)\Delta \mathbf{u} + div(\tau^e) + \mathbf{f}$$

$$We\left(\frac{\partial \tau^{e}}{\partial t} + \mathbf{u} \cdot \nabla \tau^{e} - \tau^{e} \nabla \mathbf{u}^{T} - \nabla \mathbf{u} (\tau^{e})\right) + \tau^{e} = 2\left(\frac{\mu(|D(\mathbf{u})|)}{\mu_{0}} - (1 - \alpha)\right) D(\mathbf{u}),$$

 $\alpha = \frac{\mu_e}{\mu_0} \dots$  elastic part of the total viscosity  $\mu = \mu(|D(\boldsymbol{u})|)$ 

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• flow characteristic: Weissenberg number  $We = \frac{U\lambda}{L}$  $\lambda$  characteristic relaxation time



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- flow characteristic: Weissenberg number  $We = \frac{U\lambda}{L}$  $\lambda$  characteristic relaxation time
- nonlinear coupled parabolic-hyperbolic system
- singular behaviour for large Reynolds, Weissenberg



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#### Structure equation

- assume: circular symmetry, deformation only in the radial direction
- radial wall displacement  $\eta(x_1, t) = R(x_1, t) R_0(x_1)$ ... constant w.r.t  $\theta, \theta \in [0, 2\pi)$
- linear elasticity, i.e.  $\partial \eta / \partial_{x_1} \ll 1$




• Newton law: Force = mass × acceleration

$$F = \rho_{w} h \, dc \, d\ell \times \frac{\partial^2 \eta}{\partial t^2}$$

- $\rho_W$  wall density
- h wall thickness
- dc infinitesimal length of arc  $dc = Rd\theta$
- $d\ell$  infinitesimal length in the  $x_1$ -direction
- Forces: external and internal
- 1. External forces

$$f_{ext} = f_{ext} \cdot \boldsymbol{e}_r \approx (-\mathbf{T}_f - \boldsymbol{P}_{ext}\mathbf{I})\boldsymbol{n} \cdot \boldsymbol{e}_r \, dc \, d\ell$$

 $\mathbf{T}_{\mathbf{f}}$  ... fluid Cauchy stress tensor on  $\Gamma_W := \Gamma_{W(t)}$ 





- fluid in Eulerian coordinates
- ullet structure in Langrangian coordinates  $\Longrightarrow$





- fluid in Eulerian coordinates
- ullet structure in Langrangian coordinates  $\Longrightarrow$

-transformation of the fluid stress from  $\Gamma_{W(t)}$  onto  $\Gamma_{W_0}$ :

- 
$$\Gamma_{W_0} := \{ (X_1, X_2); X_1 = x_1, X_2 = R_0(x_1) \}$$

$$-\Gamma_{W(t)} := \{(x_1, x_2); x_2 = R_0(x_1) + \eta(x_1)\}$$

 $\tilde{\eta}(X_1, X_2) = (0, \tilde{\eta}(X_1, X_2))^T = (0, \eta(x_1))^T$ 

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$$\begin{aligned} \mathbf{e}_{xt} \Big|_{\Gamma_{W_0}} &= \mathbf{f}_{ext} \cdot \mathbf{e}_r \, dc \, d\ell \\ &= -(\mathbf{T}_f + P_w \mathbf{I}) \mathbf{n} \cdot \mathbf{e}_r \frac{R}{R_0} \frac{\sqrt{1 + (\partial_{x_1} R)^2}}{\sqrt{1 + (\partial_{x_1} R_0)^2}} \, dc_0 \, d\ell_0 \\ &\approx -(\mathbf{T}_f + P_w \mathbf{I}) \mathbf{n} \cdot \mathbf{e}_r \frac{R}{R_0} \, dc_0 \, d\ell_0 \end{aligned}$$



### 2. Internal forces:

 $f_{int} = (f_{\theta} + f_{x_1}) \cdot e_r$  $f_{\theta} \dots$  internal forces due to circumferential stress  $f_{x_1} \dots$  internal forces due to longitudal stress







$$f_{\theta} \cdot \boldsymbol{e}_{r} = -E \frac{h\eta}{R_{0}R} dc_{0} d\ell_{0}$$
$$f_{x_{1}} \cdot \boldsymbol{e}_{r} = |\sigma_{x_{1}}| h \frac{\partial^{2}R}{\partial x_{1}^{2}} \left[ 1 + \left(\frac{\partial R_{0}}{\partial x_{1}}\right)^{2} \right]^{-3/2} \boldsymbol{n} \cdot \boldsymbol{e}_{r} dc_{0} d\ell_{0}$$







$$m{f}_{ heta}\cdotm{e}_{r}=-Erac{h\eta}{R_{0}R}dm{c}_{0}d\ell_{0}$$

$$\boldsymbol{f}_{x_1} \cdot \boldsymbol{e}_r = |\sigma_{x_1}| h \frac{\partial^2 R}{\partial x_1^2} \left[ 1 + \left( \frac{\partial R_0}{\partial x_1} \right)^2 \right]^{-3/2} \boldsymbol{n} \cdot \boldsymbol{e}_r dc_0 d\ell_0$$

Assuming:

$$\boldsymbol{n} \cdot \boldsymbol{e}_r \approx \left[1 + (\partial_{x_1} R_0^2)\right]^{-1/2}, \quad \eta/R \approx \eta/R_0$$

for  $|\eta| < |R_0|$ We can rewrite:

$$f_{int} = \left\{ -E \frac{h\eta}{R_0 R} + |\sigma_{x_1}| h \frac{\partial^2 R}{\partial x_1^2} \left[ 1 + \left( \frac{\partial R_0}{\partial x_1} \right)^2 \right]^{-2} \right\} dc_0 d\ell_0$$



## Structure equation



## Structure equation

$$\frac{\partial^2 \eta}{\partial t^2} - \frac{|\sigma_{x_1}|}{\rho_w} \frac{\left(\frac{\partial^2 \eta}{\partial x_1^2} + \frac{\partial^2 R_0}{\partial x_1^2}\right)}{\left[1 + \left(\frac{\partial R_0}{\partial x_1}\right)^2\right]^2} + \frac{E\eta}{\rho_w(R_0 + \eta)R_0} - c\frac{\partial^\alpha \eta}{\partial t \partial x_1^2}$$
$$= -g(R, R_0)\frac{(\mathbf{T}_f \mathbf{n} \cdot \mathbf{e}_r + P_w)}{\rho_w h}$$

- $\rho_W$  wall density
- h wall thickness
- E the Young modulus of elasticity
- $|\sigma_{x_1}| = E/3$  shear modulus
- c viscoelastic constant

$$-g(R,R_0) = rac{R_0 + \eta}{R_0} rac{\sqrt{1 + (\partial_{x_1}R)^2}}{\sqrt{1 + (\partial_{x_1}R_0)^2}}$$



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Modelling in Hemodynamics



# Fluid-domain interaction, decoupling

• fluid and geometry are coupled



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# Fluid-domain interaction, decoupling

- fluid and geometry are coupled
  - Dirichlet boundary condition

$$\boldsymbol{u}(\boldsymbol{x}_1, \boldsymbol{R}_0 + \eta, t) = \frac{\partial \eta}{\partial t} \boldsymbol{n} \quad \text{on } \Gamma^{\boldsymbol{w}},$$
 (1)

*n* is unit outward normal to the domain boundary





# Fluid-domain interaction, decoupling

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 (1)

 $\boldsymbol{n}$  is unit outward normal to the domain boundary

$$\mathbf{T}_{S}\boldsymbol{n} = \boldsymbol{g}(\boldsymbol{R},\boldsymbol{R}_{0})\mathbf{T}_{f}\boldsymbol{n}$$

the equation for domain deformation (1).

2



## Further B.C.

•  $\Gamma_{in} \ldots$  inflow conditions

$$u_{2}(0, x_{2}, t) = 0,$$
  
$$\left(2\mu(|D(\boldsymbol{u})|)\frac{\partial u_{1}}{\partial x_{1}} - p + P_{in} - \frac{\rho}{2}|u_{1}|^{2}\right)(0, x_{2}, t) = 0$$

 $0 < x_2 < R_0(0), 0 < t < T; P_{in} = P_{in}(x_2, t)$  given;  $\Gamma_{out}$  analogous

• Γ<sub>c</sub> ... flow symmetry conditions

$$u_2(x_1, 0, t) = 0$$
,  $\mu(|D(\boldsymbol{u})|) \frac{\partial u_1}{\partial x_2}(x_1, 0, t) = 0$ 

 $0 < x_1 < L, 0 < t < T$ 



## • initial conditions:

$$u(x_1, x_2, 0) = 0$$
 for any  $0 < x_1 < L$ ,  $0 < x_2 < R_0(x_1)$ 





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### conditions for structure

$$\eta(0, t) = \eta(L, t) = 0$$
  
$$\eta_{x_1}(0, t) = \eta_{x_1}(L, t) = 0$$
  
$$\eta(x_1, 0) = \frac{\partial \eta}{\partial t}(x_1, 0) = 0$$

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# I. Analysis





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Modelling in Hemodynamics

 local existence of the strong solutions:
 B. da Veiga ('04) coupling of the 2D Navier-Stokes eqs. & viscoelastic plate (friction αηtxx)







local existence of the strong solutions:

 B. da Veiga ('04)
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 Coutand, Shkoller, Cheng ('05, '06, '07)
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solution: Guidoboni, Guidorzi, Padula ('10) coupling of the 2D Navier-Stokes eqs. & elastic or viscoelastic plate (friction  $\alpha\eta_{txx}$ )



5 Čanić, Guidoboni et al. ('06) reduced structural model: viscoelastic Koiter model

$$\rho_{w}h\frac{\partial^{2}\eta}{\partial t^{2}} - C_{1}\frac{\partial^{2}\eta}{\partial x^{2}} + C_{2}\frac{\partial^{4}\eta}{\partial x^{4}} + C_{0}\eta + D_{0}\frac{\partial\eta}{\partial t} - D_{1}\frac{\partial^{3}\eta}{\partial t\partial x^{2}} + D_{2}\frac{\partial^{5}\eta}{\partial t\partial x^{4}} = f$$

-multiscale analysis of the FSI problem





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-multiscale analysis of the FSI problem

- all of these results are for Newtonian fluid rheology



Modelling in Hemodynamics

# Non-Newtonian rheology

 $\begin{array}{lll} \checkmark & \text{We assume existence of } \mathcal{U} \in C^2(\mathbb{R}^{2 \times 2}) \\ & \frac{\partial \mathcal{U}(\eta)}{\partial \eta_{ij}} &= \tau_{ij}(\eta) \qquad \mathcal{U}(0) = \frac{\partial \mathcal{U}(0)}{\partial \eta_{ij}} = 0 \\ & \frac{\partial^2 \mathcal{U}(\eta)}{\partial \eta_{mn} \partial \eta_{rs}} \xi_{mn} \xi_{rs} &\geq C_1 (1 + |\eta|)^{p-2} |\xi|^2 \\ & \left| \frac{\partial^2 \mathcal{U}(\eta)}{\partial \eta_{ij} \partial \eta_{kl}} \right| &\leq C_2 (1 + |\eta|)^{p-2}. \end{array}$ 

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Non-linear viscous term: Carreau model, power law model

$$(oldsymbol{u},oldsymbol{\psi})) = \int_{\Omega(\eta(t))} au_{ij}(D(oldsymbol{u})) D(oldsymbol{\psi}), \quad au_{ij}(D(oldsymbol{u}))) = \mu(|D(oldsymbol{u})|) D_{ij}(oldsymbol{u})$$



• ((  $\cdot$  ,  $\cdot$  )) defines a monotone and coercive operator - *p*- structure

$$((\boldsymbol{u}, \cdot)): L^{p}(0, T; \boldsymbol{W}^{1,p}(\Omega)) \to L^{p'}\left(0, T; (\boldsymbol{W}^{-1,p'}(\Omega))\right)$$

•  $((\boldsymbol{u}, \cdot))$  interplays with the convective term  $\boldsymbol{u} \cdot \nabla \boldsymbol{u}$ 

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- $((\cdot, \cdot))$  defines a monotone and coercive operator - *p*- structure
- $((\boldsymbol{u}, \cdot))$  interplays with the convective term  $\boldsymbol{u} \cdot \nabla \boldsymbol{u}$

$$\int_0^T \int_{\Omega} \boldsymbol{u} \cdot \nabla \boldsymbol{u} \, \boldsymbol{\varphi} \leq \boldsymbol{C} \qquad \Longleftrightarrow \qquad \boldsymbol{p} \geq 11/5(3D); \ \boldsymbol{p} \geq 3/2(2D)$$

first energy estimates:

$$\max_{t \in (0,T]} \|\boldsymbol{u}^n\|_{L^2(\Omega)}^2 + \int_0^T \int_\Omega \|D(\boldsymbol{u}^n)\|^p \leq C$$



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limiting process

 $\lim_{n\to\infty}\int_0^T((\boldsymbol{u}^n,\boldsymbol{\psi}))$ 

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limiting process

$$\lim_{n\to\infty}\int_0^T((\boldsymbol{u}^n,\psi))$$

- theory of monotone operators: Ladyzhenskaja, Lions (existence of weak solutions)  $p \ge \frac{11}{5}$  (3D),  $p \ge 2$  (2D) (Dirichlet B.C.)



# Existence of the non-Newtonian fluids in a fixed bdd. domain

-testing by ∆*u* & Vitali theorem Nečas, Málek, Ržička, et al. ('93-01)

- existence of global weak solutions for p > 9/5 (3D unsteady, per. BC)

- existence of local strong solutions for  $p \ge 5/3$  (3D unsteady, per. BC)

- existence of global weak solutions for  $p \in [2,3)$  (3D unsteady, Dir. BC)

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- existence of global weak solutions for  $p \in [2,3)$  (3D unsteady, Dir. BC)
- $L^{\infty}$ -truncation

Frehse, Málek, Steinhauer, Ružička ('97, '99) existence of global weak solutions for p > 8/5 (3D unsteady, Dir. BC)



# Existence of the non-Newtonian fluids in a fixed bdd. domain

- testing by ∆*u* & Vitali theorem Nečas, Málek, Ržička, et al. ('93-01)
- existence of global weak solutions for p > 9/5 (3D unsteady, per. BC)
- existence of local strong solutions for  $p \ge 5/3$  (3D unsteady, per. BC)
- existence of global weak solutions for  $p \in [2,3)$  (3D unsteady, Dir. BC)
- $L^{\infty}$ -truncation

Frehse, Málek, Steinhauer, Ružička ('97, '99) existence of global weak solutions for p > 8/5 (3D unsteady, Dir. BC)

• Diening, Ružička et al. ('05,'07):

existence of local strong solutions for p > 7/3 (3D unsteady, per.BC)



# Existence results ... continue

- local pressure method Wolf ('07)
- existence of global weak solutions for p > 8/5 (3D unsteady, Dir. BC), p > 3/2 (2D)





## Existence results ... continue

- local pressure method Wolf ('07)
- existence of global weak solutions for  $\rho>8/5$  (3D unsteady, Dir. BC),  $\rho>3/2$  (2D)
- Lipschitz-truncation & local pressure method
- Diening, Ružička, Wolf ('10):

existence of global weak solutions p > 6/5 (3D unsteady, Dir. BC), p > 1 (2D)



# FSI for non-Newtonian fluids

Theorem (M.L., Hundertmark, Nečasová ('11))

Let  $p \ge 2$ . Assume  $P|_{in,out,w} \in L^{p'}(0, T; L^2(\partial \Omega))$ . Then  $\exists (\boldsymbol{u}, \eta)$  a weak solution of the nonlinear FSI problem, s.t.

$$\begin{split} & \boldsymbol{u} \in L^p(0,\,T;\,\boldsymbol{W}^{1,p}(\Omega(\eta(t)))) \cap L^\infty(0,\,T;\,L^2(\Omega(\eta(t)))) \\ & \eta \in \,\boldsymbol{W}^{1,\infty}(0,\,T;\,L^2(0,L)) \cap \,H^1(0,\,T;\,H^2_0(0,L)). \end{split}$$

 $\gamma_{\eta(t)}(\textbf{\textit{u}}) = (\textbf{0},\eta_t) \text{ on } \Gamma_{w}$ 

 $div(\mathbf{u}) = 0$  a.e. on  $\Omega(\eta(t))$  and the corresponding integral identity of the weak formulation holds.


## Weak formulation - problem $\mathcal{P}$

$$\int_{0}^{T} \int_{\Omega(\eta(t))} \left\{ -\rho \boldsymbol{u} \cdot \frac{\partial \varphi}{\partial t} + ((\boldsymbol{u}, \varphi)) + \rho \sum_{i,j=1}^{2} u_{i} \frac{\partial u_{j}}{\partial x_{i}} \varphi_{j} \right\}$$
  
$$\pm \int_{0}^{T} \int_{\Gamma_{in,out}} \left( P_{in,out} - \frac{\rho}{2} |u_{1}|^{2} \right) \varphi_{1} + \int_{0}^{T} \int_{\Gamma_{w}} P_{w} \varphi_{2}$$
  
$$+ \int_{0}^{T} \int_{0}^{L} \left( -\frac{\partial \eta}{\partial t} \frac{\partial \xi}{\partial t} + c \frac{\partial^{3} \eta}{\partial x_{1}^{2} \partial t} \frac{\partial^{2} \xi}{\partial x_{1}^{2}} + a \frac{\partial \eta}{\partial x_{1}} \frac{\partial \xi}{\partial x_{1}} + b \eta \xi \right) = 0$$

for every test functions

$$\begin{split} \varphi(x_1, x_2, t) &\in H^1(0, T; W^{1, p}(\Omega(\eta(t)))) \\ \text{such that} & \text{div } \varphi = 0 \quad \text{a.e on } \Omega(\eta(t)), \\ \gamma_{\eta(t)} \varphi_2 &\in H^1(0, T; H^2_0(\Gamma_w)) \\ \xi(x_1, t) &= \varphi_2(x_1, R_0(x_1) + \eta(x_1, t), t) \end{split}$$



- Idea: approximate problem  $\mathcal{P}(\kappa,\varepsilon,k)$ 
  - Global iteration: given domain deformation  $h(x_1, t) \equiv h^{(k)}(x_1, t) = R_0(x_1) + \eta^{(k-1)}(x_1, t)$





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  - **2** Transformation of  $\Omega(h)$  to a domain  $D := (0, L) \times (0, 1)$

$$\mathbf{v}(y_1, y_2, t) \equiv \mathbf{u}(y_1, h(y_1, t)y_2, t); 
 q(y_1, y_2, t) \equiv \rho^{-1} \pi(y_1, h(y_1, t)y_2, t); 
 \sigma(y_1, t) \equiv \frac{\partial \eta(y_1, t)}{\partial t}$$



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Split the structure equation into two steps:

$$-\mathbf{T}_{f}\boldsymbol{n}\cdot\boldsymbol{e}_{r}-\boldsymbol{P}_{w}-\frac{\rho}{2}\boldsymbol{u}_{2}\left(\boldsymbol{u}_{2}-\frac{\partial\eta^{(k-1)}}{\partial t}\right)=\boldsymbol{\kappa}\rho\left(\frac{\partial\eta}{\partial t}-\boldsymbol{u}_{2}\right)$$



Idea: approximate problem P(κ, ε, k)
 Global iteration: given domain deformation h(x<sub>1</sub>, t) ≡ h<sup>(k)</sup>(x<sub>1</sub>, t) = R<sub>0</sub>(x<sub>1</sub>) + η<sup>(k-1)</sup>(x<sub>1</sub>, t)

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$$o_{w}h\left[\frac{\partial^{2}\eta}{\partial t^{2}}-a\frac{\partial^{2}(\eta+R_{0})}{\partial x_{1}^{2}}+b\eta-c\frac{\partial^{5}\eta}{\partial t\partial x_{1}^{4}}\right]=\kappa\left(\frac{\partial\eta}{\partial t}-u_{2}\right)$$



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#### Reason:

by  $\kappa \longrightarrow \infty$  we obtain  $\partial_t \eta = u_2$ , which is original Dirichlet condition

Modelling in Hemodynamics



Idea: approximate problem P(κ, ε, k)
 Global iteration: given domain deformation h(x<sub>1</sub>, t) ≡ h<sup>(k)</sup>(x<sub>1</sub>, t) = R<sub>0</sub>(x<sub>1</sub>) + η<sup>(k-1)</sup>(x<sub>1</sub>, t)

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Approximation of the incompressibility condition by pseudo-compressibility

$$\varepsilon \frac{\partial \boldsymbol{p}}{\partial t} - \varepsilon \Delta \pi + \operatorname{div} \boldsymbol{u}_{\varepsilon} = \boldsymbol{0}.$$



# Idea of the proof

- Construct Galerkin approximations to the approximate problem P(κ, ε, k)
- Apriori estimates implies (independent on ε, κ) for a fixed h(x<sub>1</sub>, t)
- Limiting process in the Galerkin approximations: Lions-Aubin & Minty-Browder for convergence in nonlinear terms
- 3 Limiting process ε → 0, κ → ∞ for fixed h(x<sub>1</sub>, t) problem P(k)
- Schauder fixed point arguments original problem *P* on Ω(η(t))

